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(54) **SYSTEMS AND METHODS FOR ENHANCED DISTRIBUTION OF A BIOLOGIC AGENT WITHIN THE BRAIN AND SPINAL CORD**

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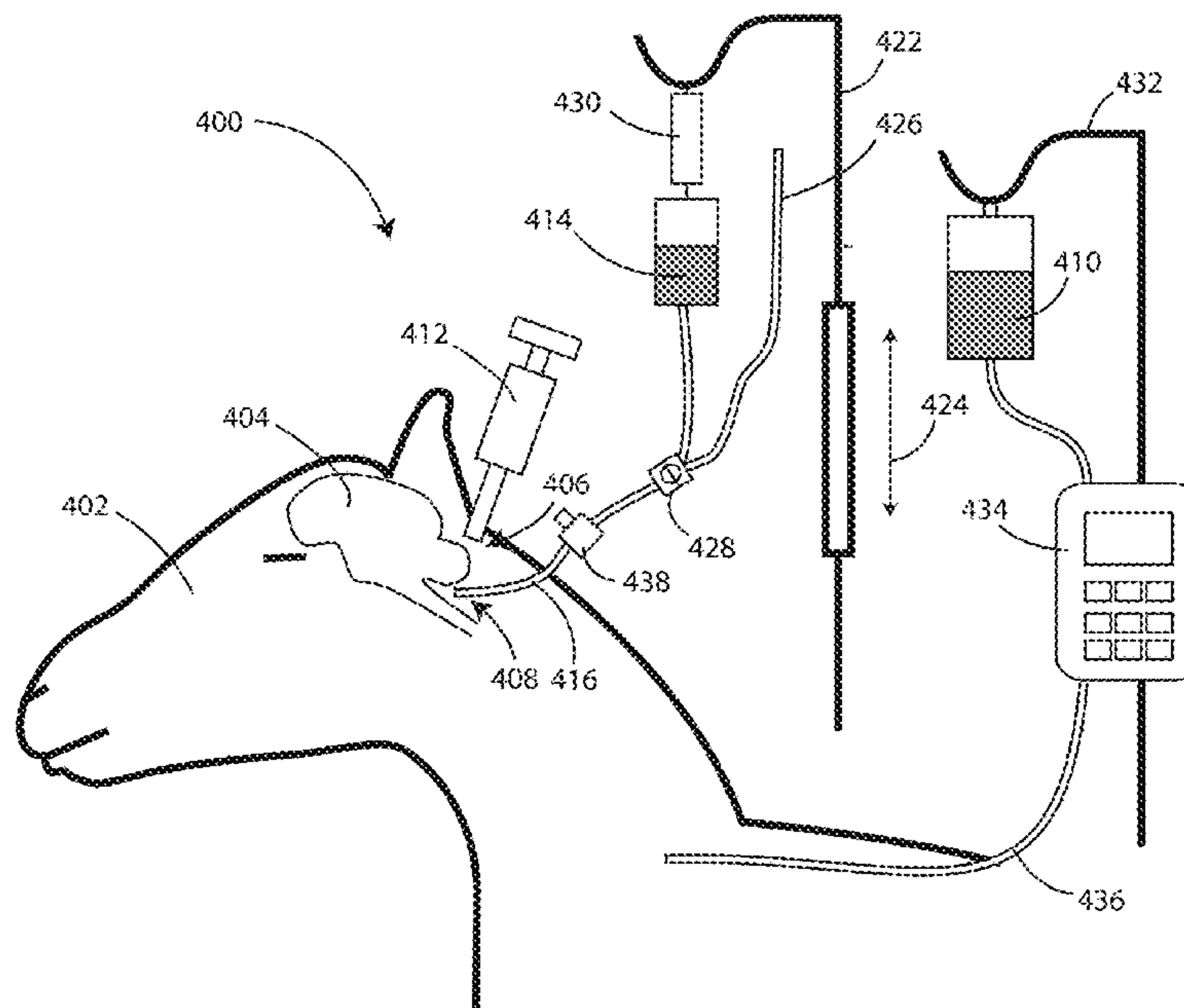
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(57) **ABSTRACT**

Aspects herein relate to systems and methods for delivery of biologic agents to the central nervous system. In various embodiments, a method of administering a therapeutic agent to the central nervous system (CNS) is included. The method can include injecting a therapeutic agent into a first cerebrospinal fluid (CSF) region of the subject. The method can further include establishing fluid communication between a fluid reservoir and a second cerebrospinal fluid (CSF) region of a subject, the fluid having a hydraulic pressure at or above an intracranial pressure. The method can further include infusing a hyperosmotic fluid systemically. Other embodiments, including kits and systems are also included herein.

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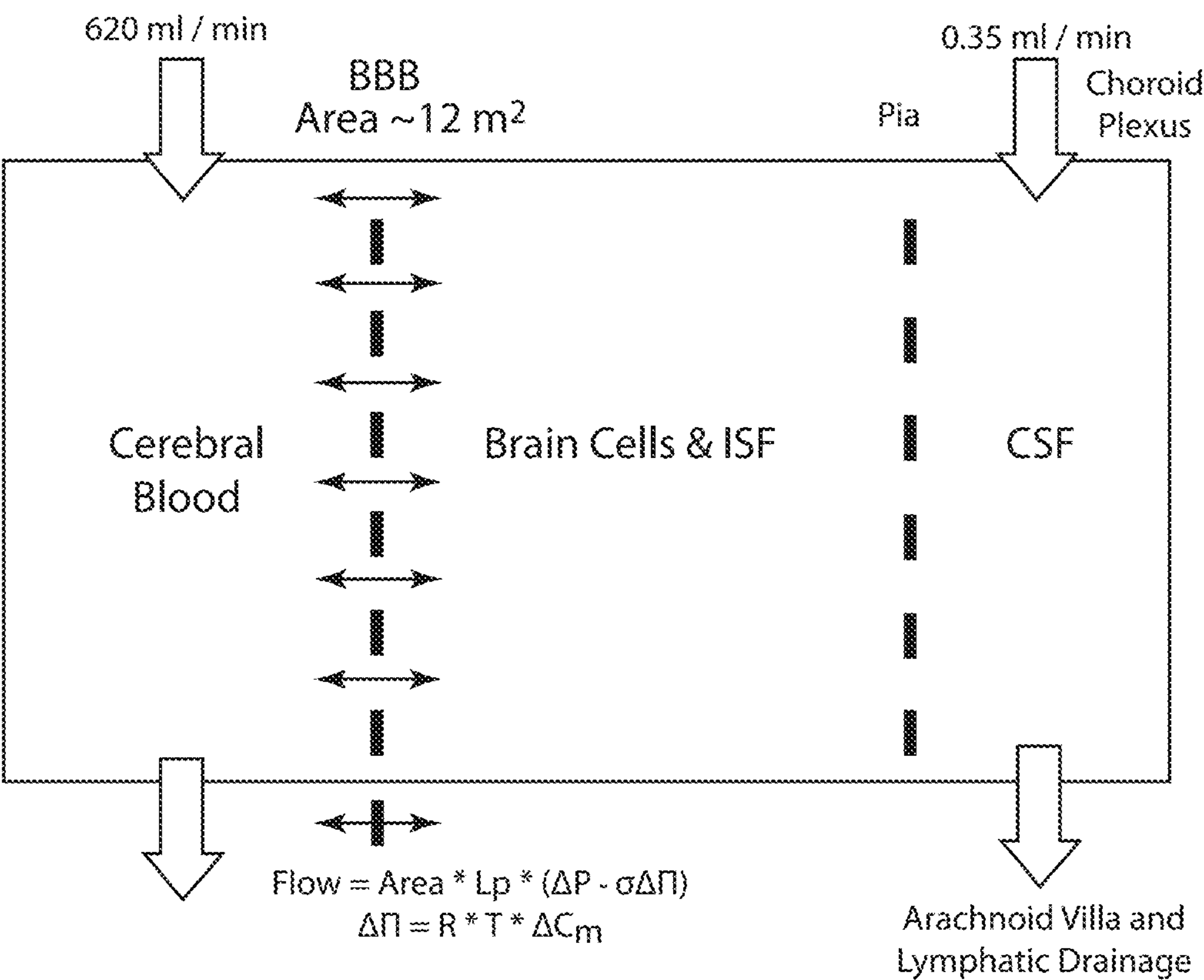


FIG. 1

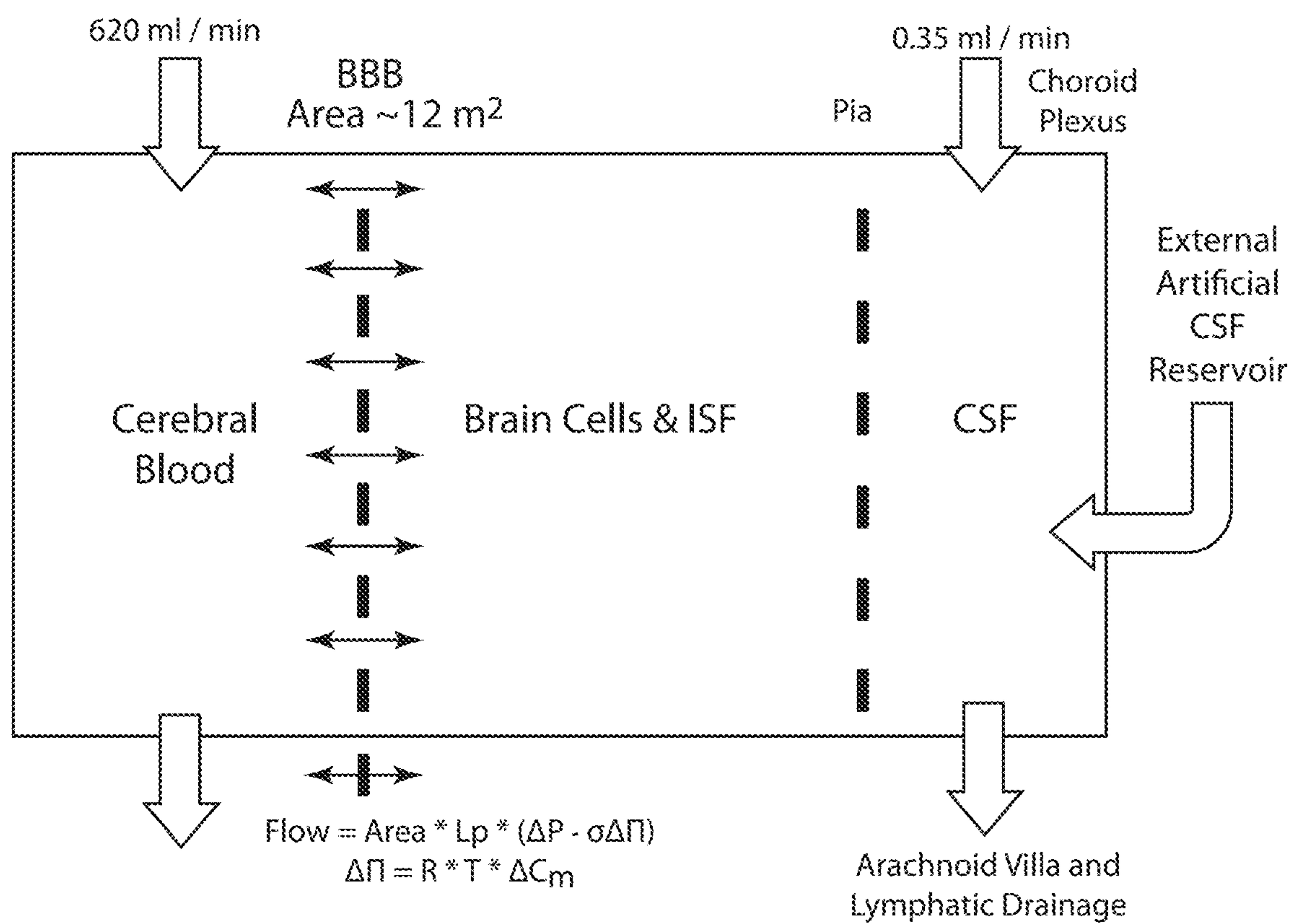


FIG. 2

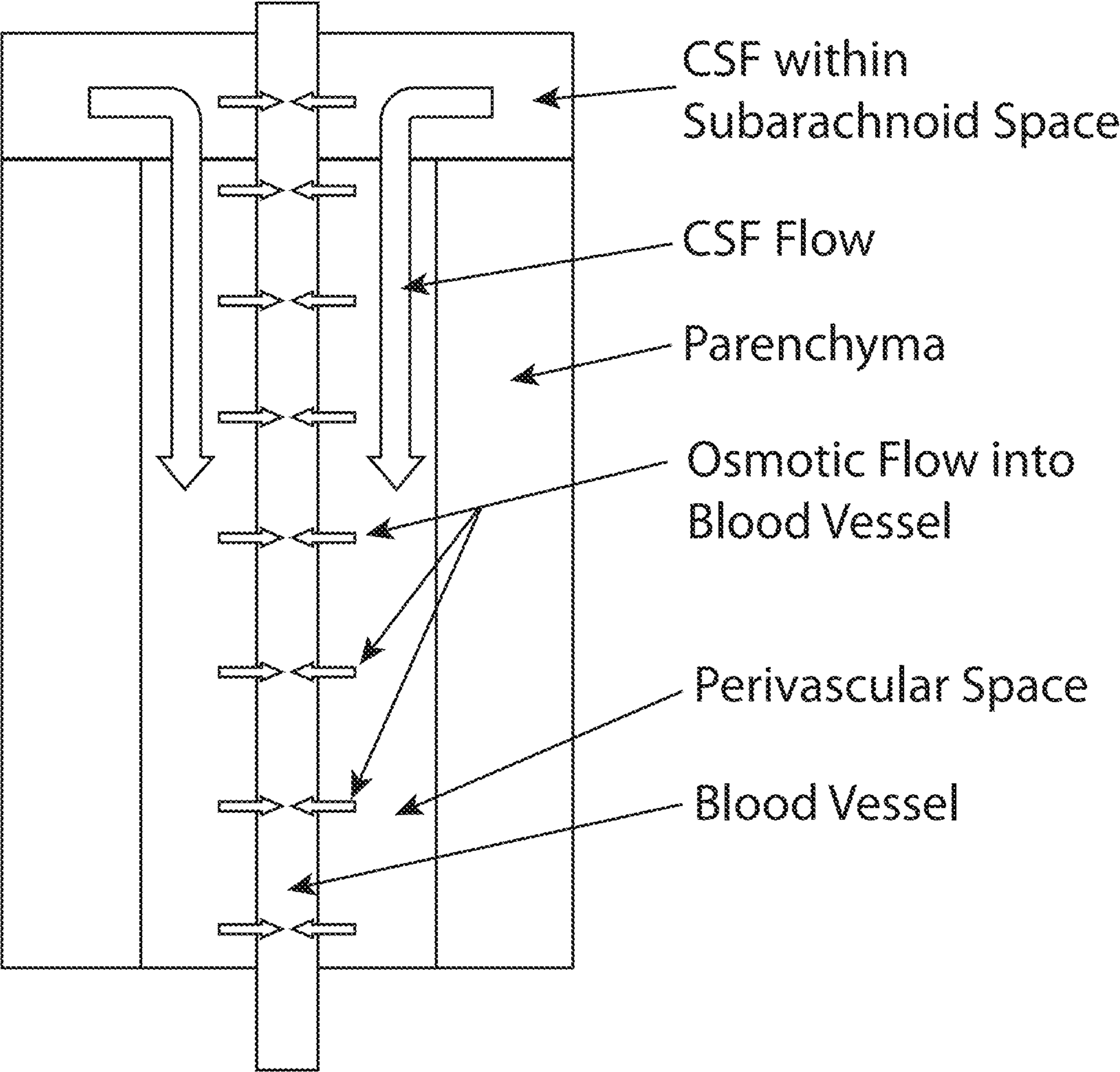


FIG. 3

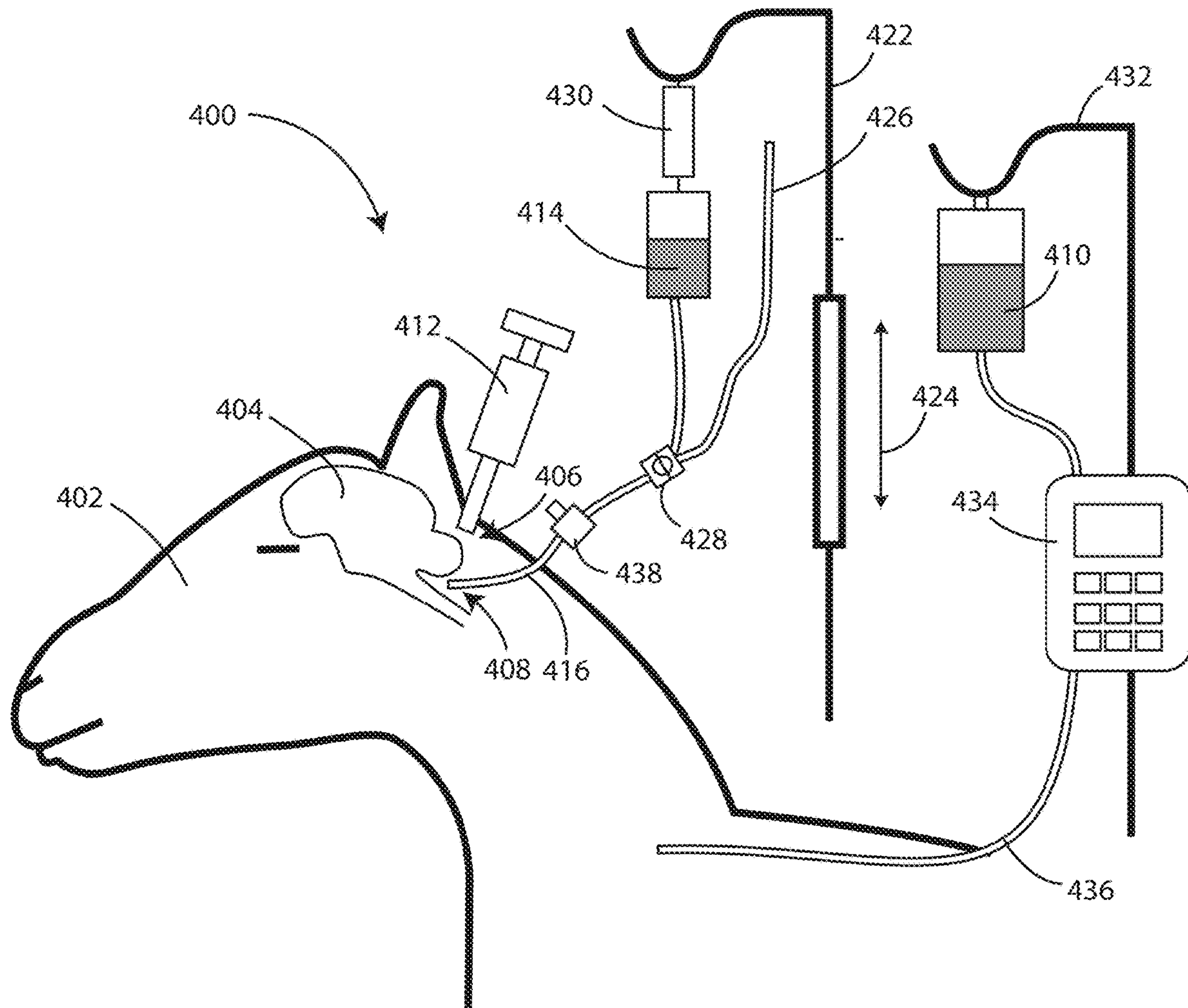


FIG. 4

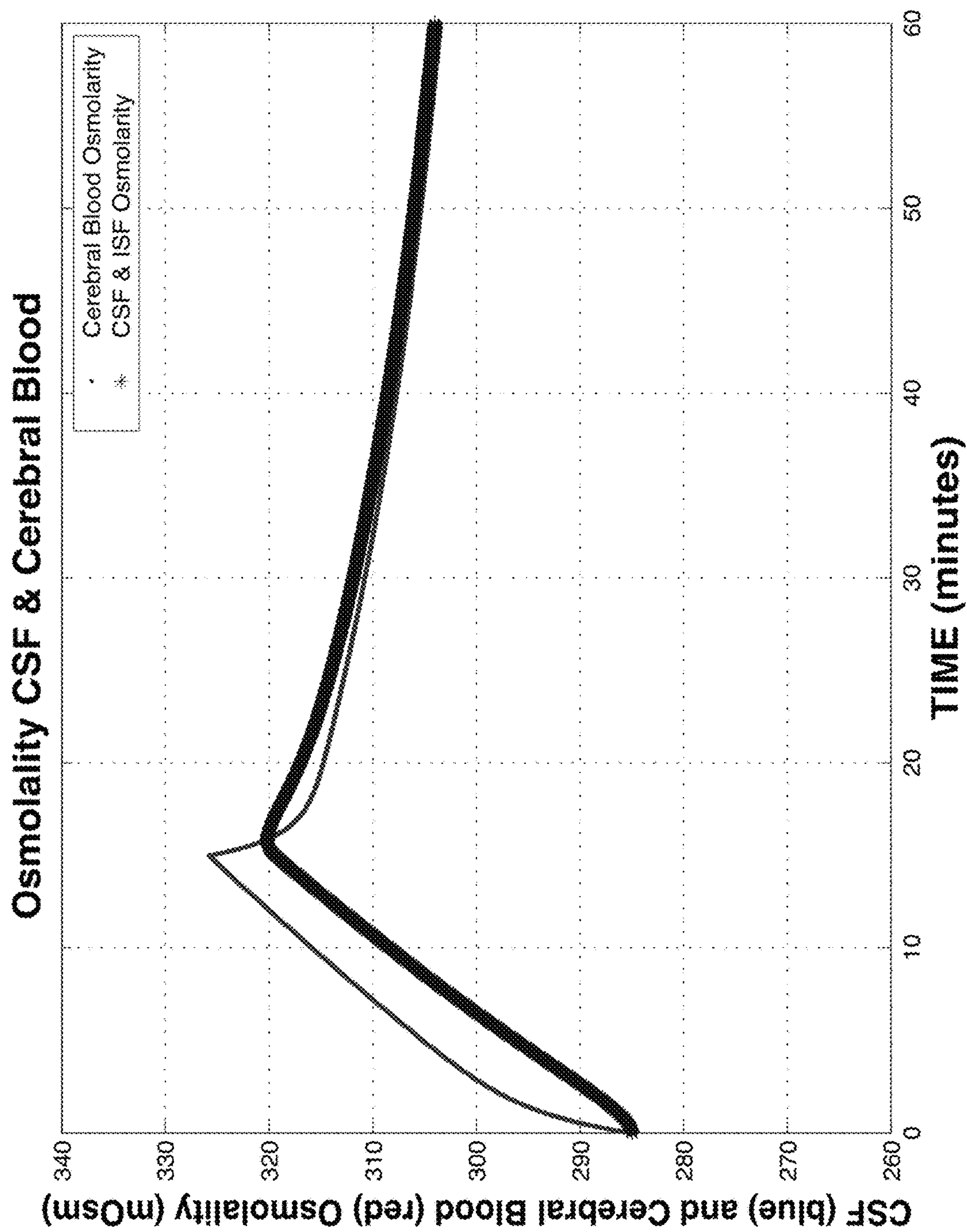


FIG. 5A

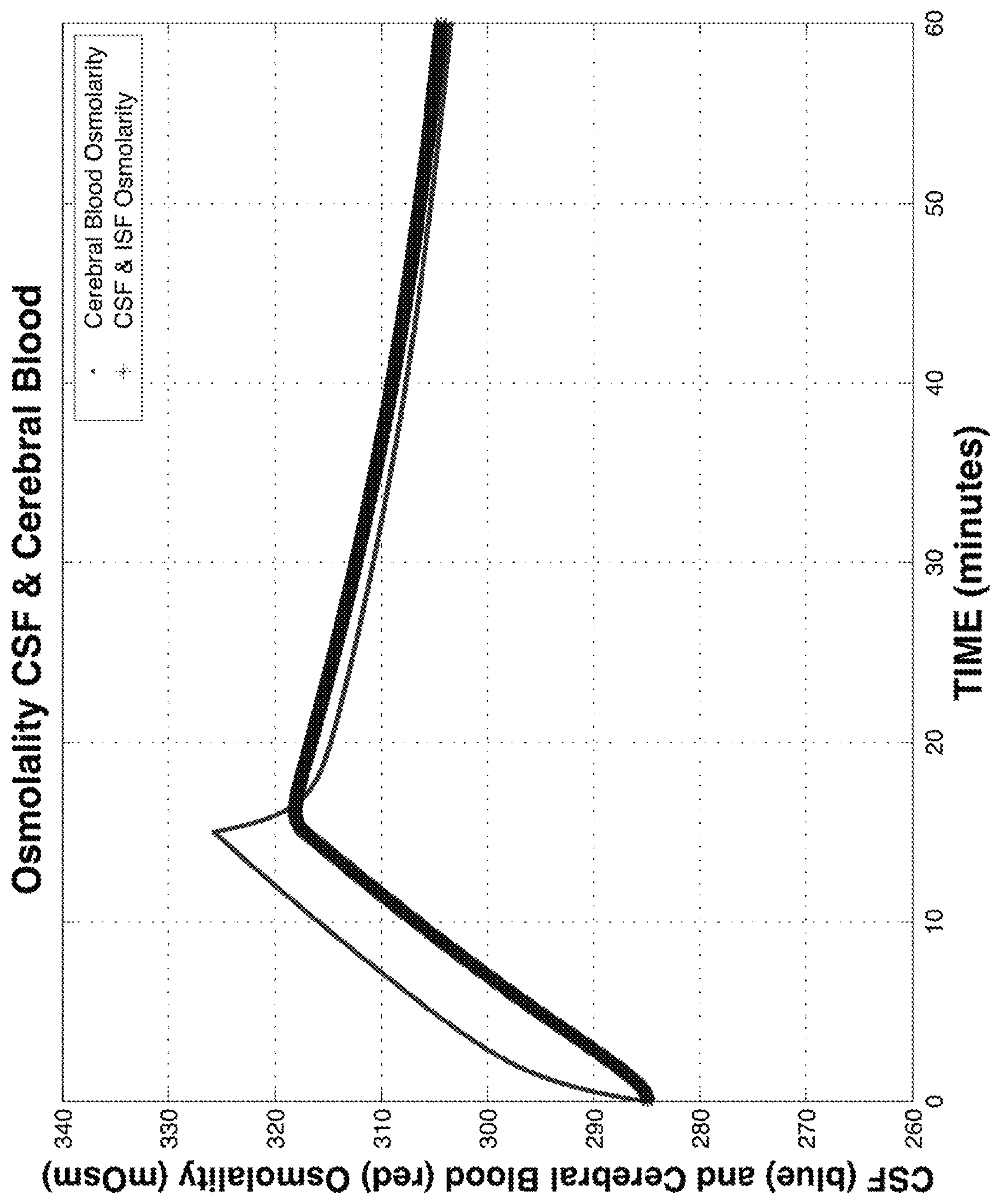


FIG. 5B

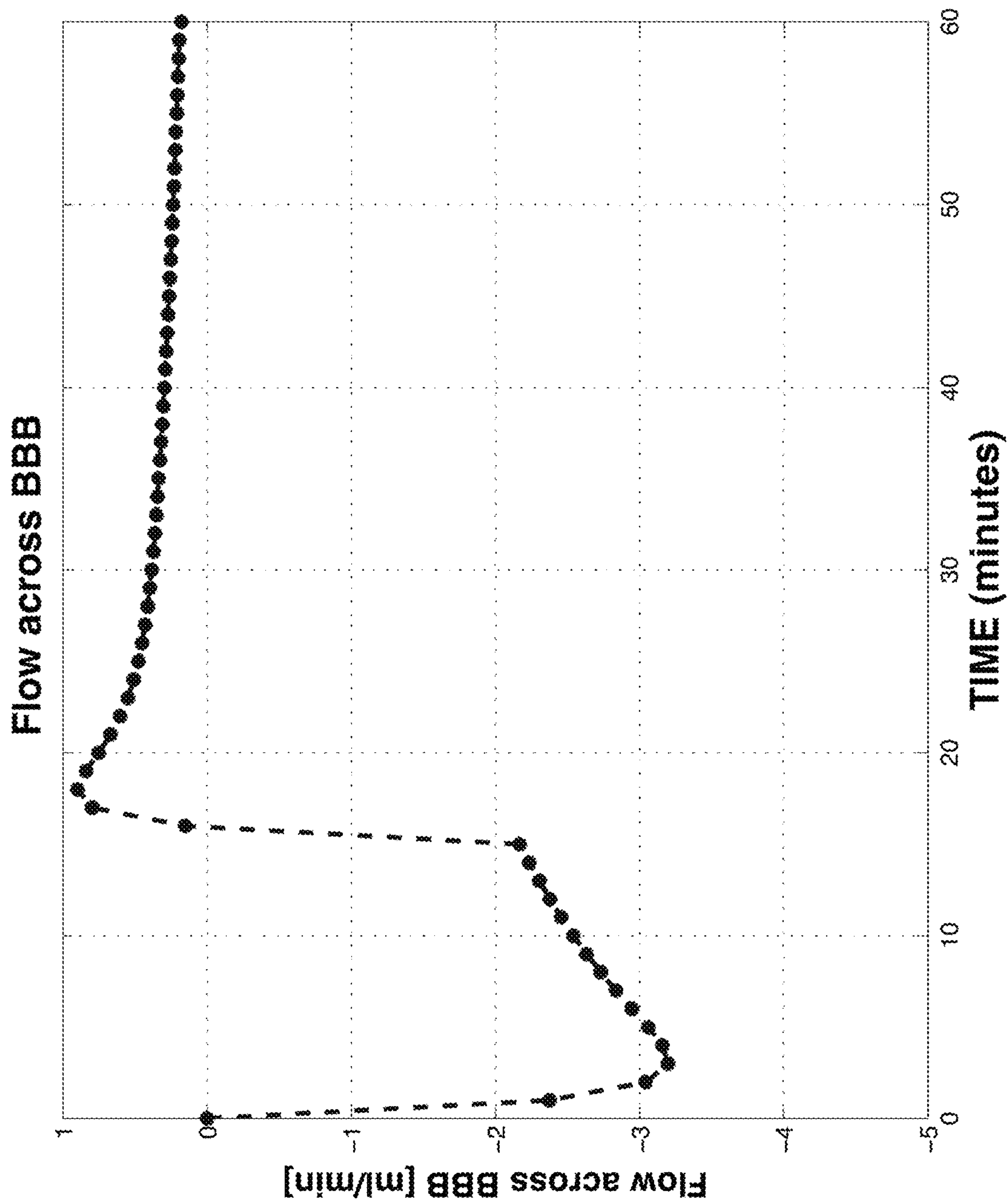


FIG. 5C

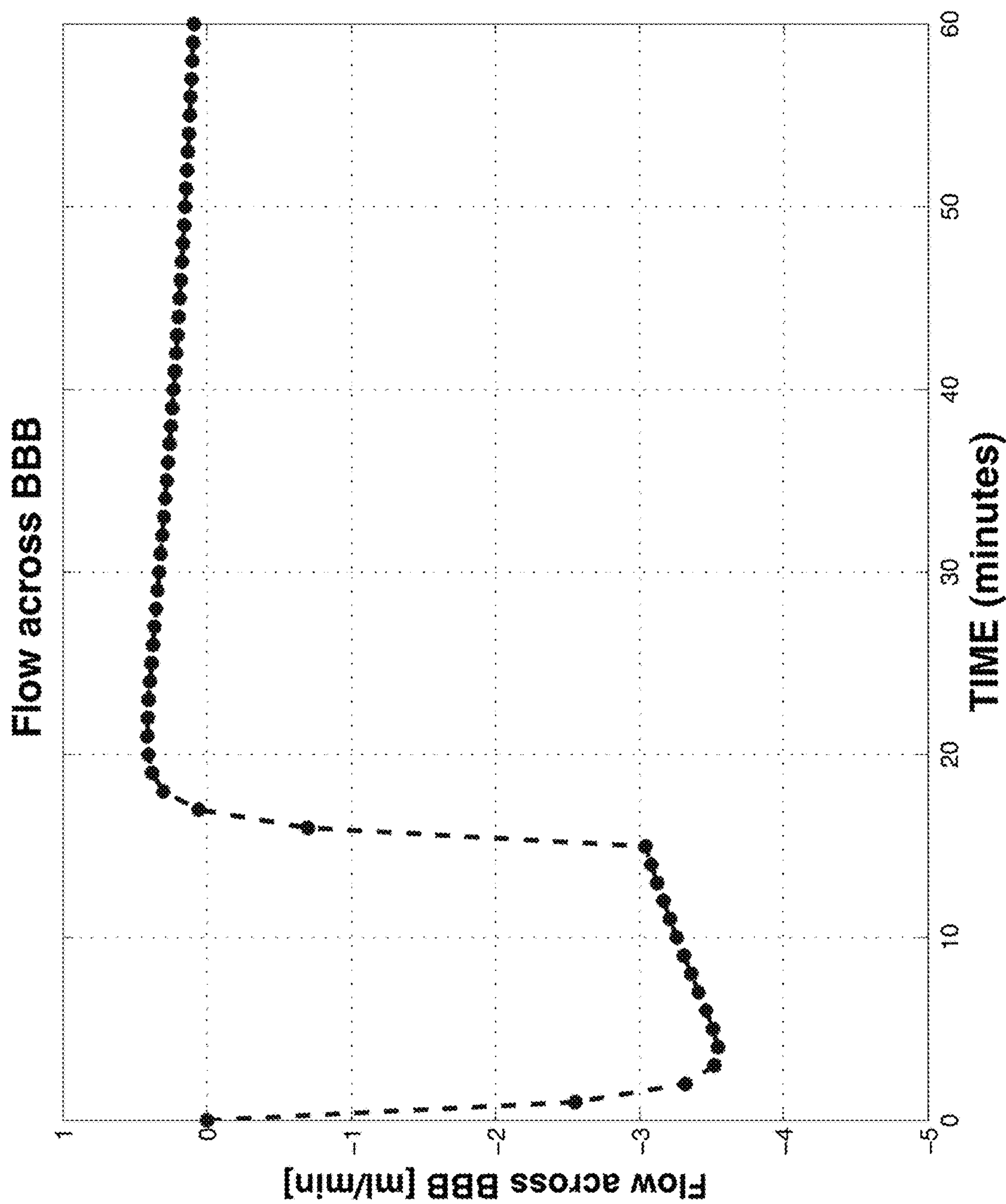


FIG. 5D

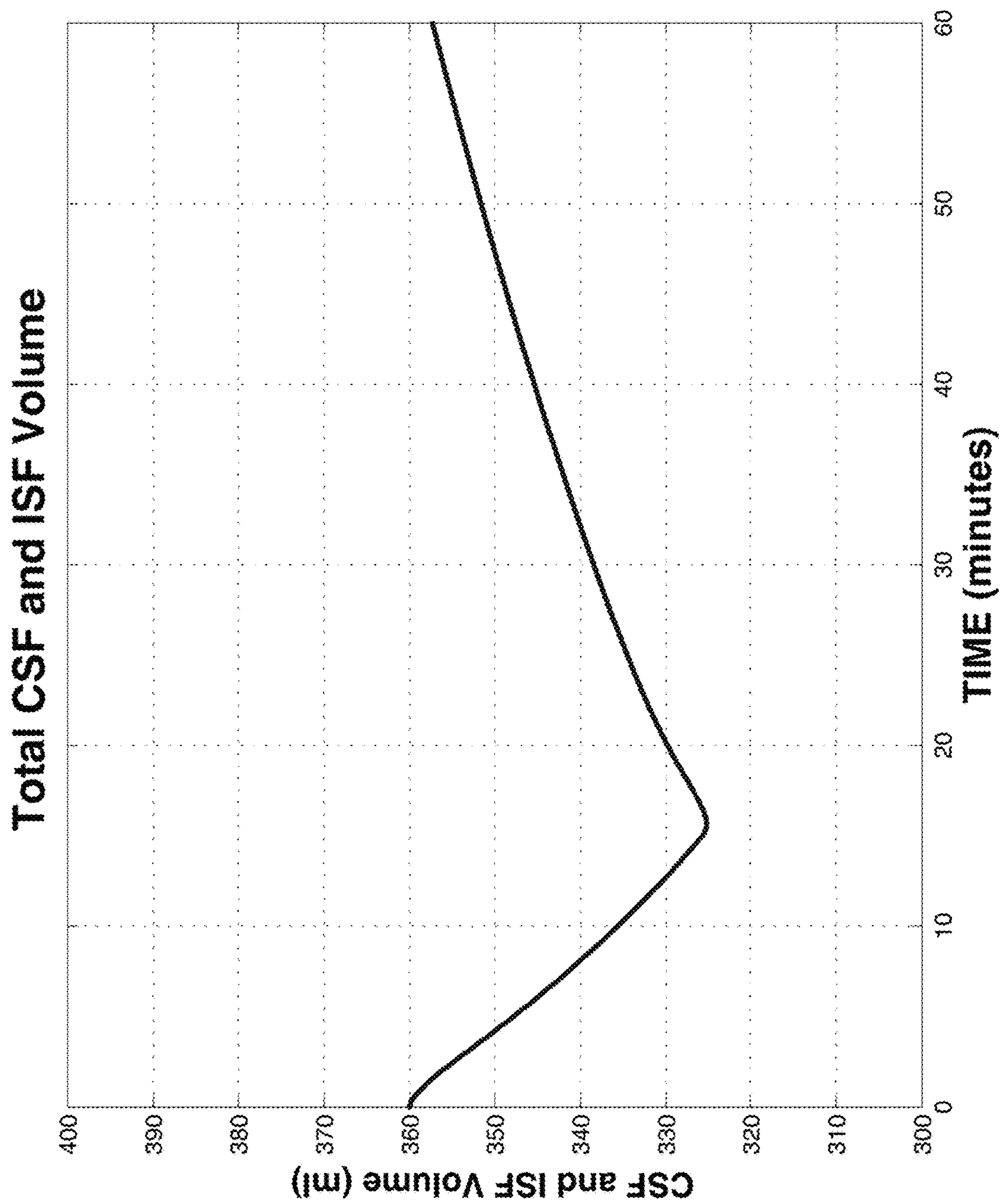


FIG. 6A

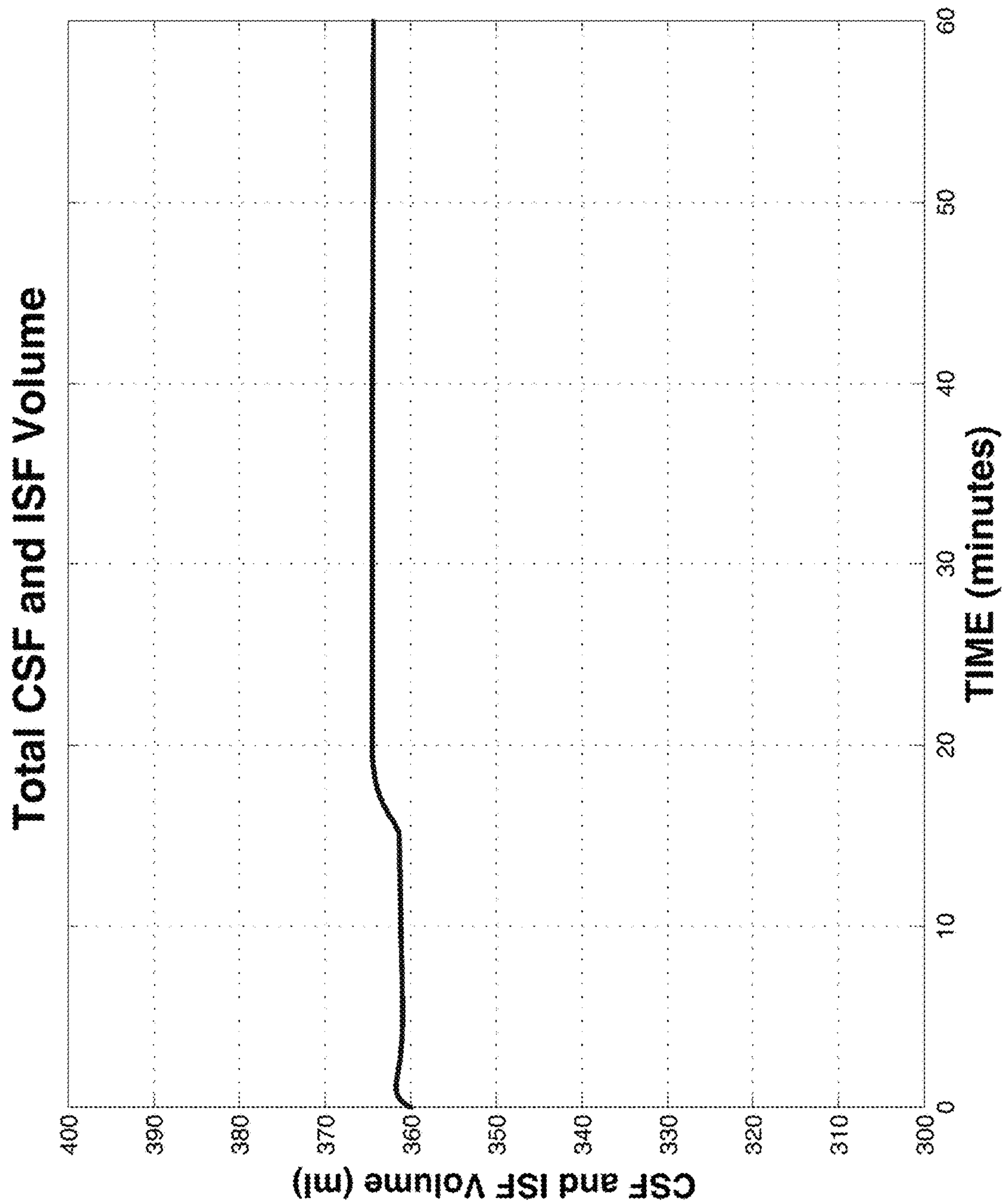


FIG. 6B

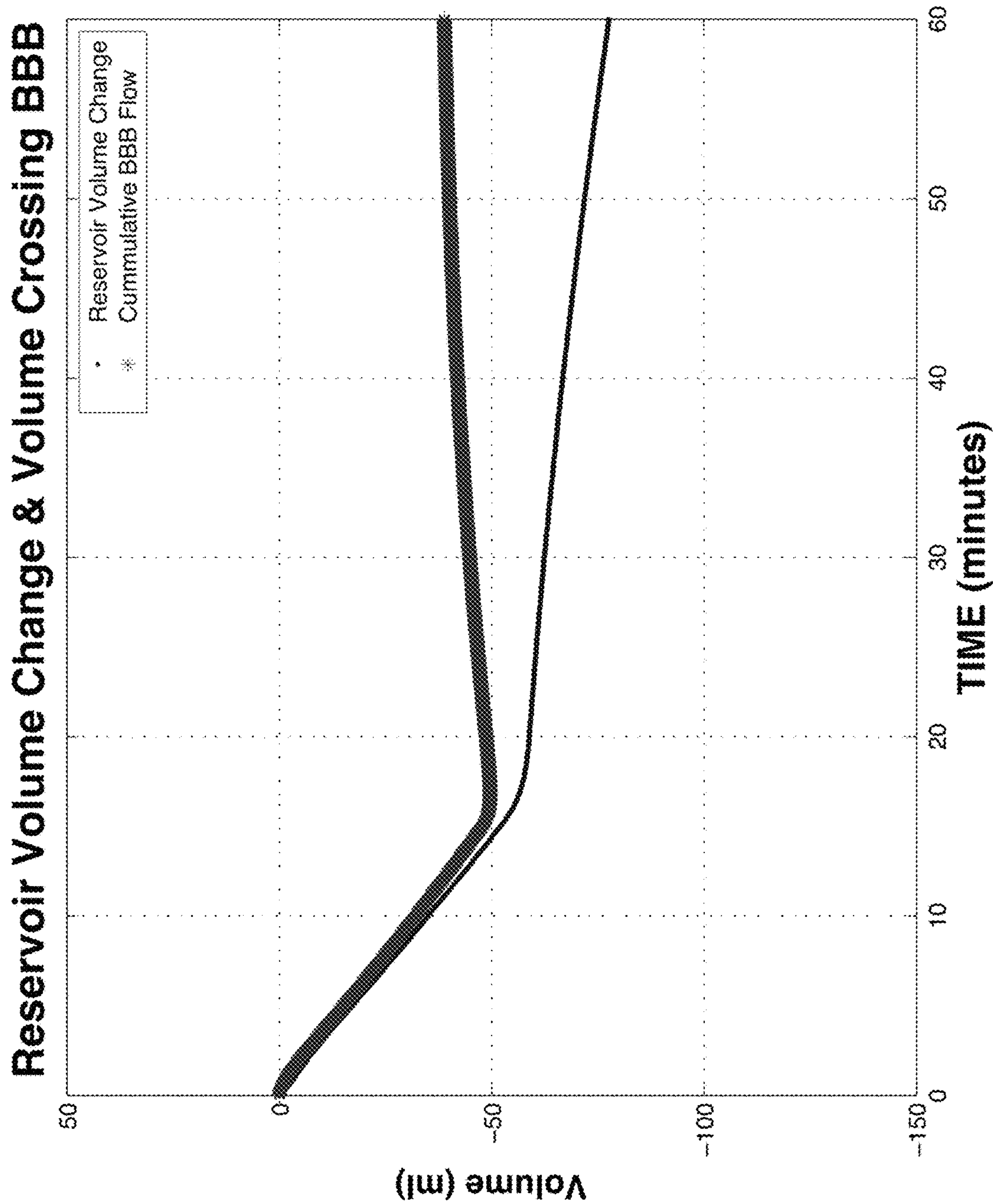


FIG. 6C

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SYSTEMS AND METHODS FOR ENHANCED DISTRIBUTION OF A BIOLOGIC AGENT WITHIN THE BRAIN AND SPINAL CORD

This application claims the benefit of U.S. Provisional Application No. 62/456,281, filed Feb. 8, 2017, the content of which is herein incorporated by reference in its entirety.

FIELD

Aspects herein relate to systems and methods for delivery of biologic agents to the central nervous system and, more particularly, for enhanced distribution of therapeutic macromolecules and particles, including polynucleotides and proteins, genetic vectors, and cells, to the brain and spinal cord parenchyma.

BACKGROUND

The improved understanding of the genetic basis of many neurological diseases and advancements in biotechnology are leading to the development of new therapeutic agents including polynucleotides and polypeptides that are able to precisely target the underlying cause of disease. In addition, animal studies and initial clinical investigations have shown that in-vivo gene vector transfer with chronic expression of these therapeutic agents enables long-term amelioration of disease (Weinberg, Samulski et al. 2013, Hocquemiller, Giersch et al. 2016, Karumuthil-Melethil, Nagabhushan Kalburgi et al. 2016, Osmon, Woodley et al. 2016). Alternatively, ex-vivo gene therapy, involving the genetic modification of cells outside the body that are then being delivered to affected tissue within the patient, has also resulted in long term benefit in the treatment of disease (Cartier, Hacein-Bey-Abina et al. 2009). These polynucleotides, polypeptides, gene vectors, and altered biologic cells are generally classified as biologic agents. The particle sizes of these biologic macromolecules, vector capsids, and cells are significantly larger than traditional pharmaceutical medications. This larger particle size diminishes diffusion transport and membrane permeability characteristics of these agents within biological systems compared to the traditional small-molecule therapeutic agents.

SUMMARY

Aspects herein relate to systems and methods for delivery of biologic agents to the central nervous system. In various embodiments, a method of administering a therapeutic agent to the central nervous system (CNS) is included. The method can include injecting a therapeutic agent into a first cerebrospinal fluid (CSF) region of the subject. The method can further include establishing fluid communication between a fluid reservoir and a second cerebrospinal fluid (CSF) region of a subject, the fluid having a hydraulic pressure at or above an intracranial pressure. The method can further include infusing a hyperosmotic fluid systemically.

In some embodiments, a kit is included. The kit can include a first reservoir and a first fluid configured to be disposed within the first reservoir. The first fluid can be isotonic or hypotonic. The kit can further include an instrument for injecting a therapeutic agent into a first CSF space. The kit can further include a conduit for providing fluid communication between the first reservoir and a second CSF space. The kit can further include a second reservoir and a second fluid configured to be disposed within the second reservoir. The second fluid can be hyperosmotic.

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In some embodiments, a system is included. The system can include a first reservoir and a first fluid disposed within the first reservoir. The first fluid is isotonic or hypotonic. The system can include a conduit for providing fluid communication between the first reservoir and a second CSF space. The system can also include a second reservoir and a second fluid disposed within the second reservoir. The second fluid can be hyperosmotic.

This summary is an overview of some of the teachings of the present application and is not intended to be an exclusive or exhaustive treatment of the present subject matter. Further details are found in the detailed description and appended claims. Other aspects will be apparent to persons skilled in the art upon reading and understanding the following detailed description and viewing the drawings that form a part thereof, each of which is not to be taken in a limiting sense. The scope herein is defined by the appended claims and their legal equivalents.

BRIEF DESCRIPTION OF THE DRAWINGS

Aspects herein can be more completely understood in consideration of the following detailed description of various embodiments in connection with the accompanying drawings, in which:

FIG. 1 is a simplified multi-compartment model of the CNS illustrating the Monro-Kellie hypothesis that the CNS has a fixed volume consisting of compartments of blood, parenchyma/ISF, and CSF.

FIG. 2 is the same multi-compartment model of the CNS as shown in FIG. 1 with the addition of fluid flow connectivity from an external reservoir containing artificial CSF to the CSF compartment.

FIG. 3 is an illustration of perivascular spaces that emanate from the brain surface and provide a route of fluid flow from the CSF compartment to deep brain regions.

FIG. 4 is a schematic diagram of a system in accordance with various embodiments herein.

FIGS. 5A-5D include graphs generated from computer simulations of computer simulations of the multi-compartment model during the intravenous delivery of 20% mannitol (1 g/kg) for 15 minutes: (A) Osmolality of CSF and cerebral blood without fluid connectivity to the artificial CSF reservoir, as shown in FIG. 1; (B) Osmolality of CSF and cerebral blood with fluid connectivity to the artificial CSF reservoir, as shown in FIG. 2; (C) Fluid flow into the brain across the BBB without fluid connectivity to the artificial CSF reservoir, as shown in FIG. 1; (D) Fluid flow into the brain across the BBB with fluid connectivity to the artificial CSF reservoir, as shown in FIG. 2.

FIGS. 6A-6C include graphs generated from computer simulations of computer simulations of the multi-compartment model during the intravenous delivery of 20% mannitol (1 g/kg) for 15 minutes: (A) Total combined ISF and CSF volume without fluid connectivity to the artificial CSF reservoir, as shown in FIG. 1; (B) Total combined ISF and CSF volume with fluid connectivity to the artificial CSF reservoir, as shown in FIG. 2; (C) Reservoir volume change and cumulative fluid volume crossing the BBB with fluid connectivity to the artificial CSF reservoir, as shown in FIG. 2.

These drawings are to be considered general representations of some embodiments, and it will be appreciated that they are not drawn to encompass all embodiments, nor are they always drawn to scale. While aspects herein are susceptible to various modifications and alternative forms, specifics thereof have been shown by way of example and

drawings, and will be described in detail. It should be understood, however, that the scope herein is not limited to the particular embodiments described. On the contrary, the intention is to cover modifications, equivalents, and alternatives falling within the spirit and scope of that described herein.

DETAILED DESCRIPTION

It is identified herein that there exists an unmet need for a simple, safe, and effective means of achieving broad distribution of polynucleotides, polypeptides, gene vectors, altered biologic cells and other large particle therapeutic agents throughout a human sized brain.

As described above, the particle sizes of biologic macromolecules, vector capsids, and cells are significantly larger than traditional pharmaceutical medications. This larger particle size diminishes diffusion transport and membrane permeability characteristics of these agents within biological systems compared to the traditional small-molecule therapeutic agents.

The large particle sizes of these agents thereby present additional restraints and limitations in adequately delivering these biologic agents for treating diseases, and in particular, diseases of the central nervous system (CNS).

While some diseases are primarily localized within particular regions of the CNS, as may be the case for Parkinson's disease, many diseases affect multiple regions, or in some cases, all regions of the CNS. Examples of diseases that have a diffuse effect within the CNS include cancers, such as advanced glioblastoma multiforme, and many neurodegenerative diseases, including Alzheimer's disease, Multiple Sclerosis, and many lysosomal storage diseases. The effectiveness of biologic agents is dependent on the delivery to the disease-affected cells. It is therefore believed that these diseases that broadly affect the CNS will require that a biologic agent reach a therapeutic concentration level within correspondingly broad regions of distribution in order to be effective.

Biologic agent transport characteristics are dependent on particle size. As is generally known by the Stokes-Einstein Equation, the diffusion coefficient decreases as the particle size increases. ($D = k_B T / 6 \pi \eta r$ where D is the diffusion coefficient, k_B is Boltzmann's constant, T is the absolute temperature, η is the dynamic viscosity, and r is the radius of an equivalent spherical particle.) The effective diffusion coefficient is further diminished by smaller size and greater tortuosity of extracellular tissue channels, such as those of dense brain tissue. With a smaller diffusion coefficient, diffusion becomes a less significant factor for transport of particles within a biologic system, and the particle distribution becomes increasingly dependent on convective flow. The relative significance of convection compared to diffusion for particle transport is quantified by the Peclet number, $Pe = VL / De$, where L is the characteristic length, V the velocity, De the effective mass diffusion coefficient. Convection thereby also becomes relatively more important in the distribution of particles in large animals and humans that have a larger characteristic length compared to small animals, such as laboratory mice.

Classical pharmacokinetic (PK) theory models the distribution of small molecule pharmaceutical agents between body compartments. Classical PK theory assumes that the agents are well mixed within these compartments. The lack of significant diffusion mixing of large particle biologic agents precludes the fundamental application of classical pharmacokinetic theory within dense tissue, such as the

brain. The distribution of biologic agents within the CNS is primarily governed by the flow of fluids surrounding and within the parenchyma and is better modeled by the physics of fluid flow, fluid physiology, and the convective particle transport within porous media.

The distribution of biologic agents into the CNS must also overcome physiologic barriers. The blood-brain barrier (BBB) separates the CNS from systemic blood circulation. This barrier is composed of a capillary endothelial layer and tightly associated accessory cells (pericytes, astrocytes). The BBB limits transport of large, hydrophilic molecules and cells from entering the CNS. The exception is for some specific proteins such as transferrin, lactoferrin and low-density lipoproteins, which are taken up by receptor-mediated endocytosis. Small molecule pharmaceutical agents depend on active or non-active transport across the BBB to reach the CNS, but the BBB is generally impervious to most biologic agents.

Multiple methods have been previously investigated for biologic agents to either overcome or bypass the BBB and enter the CNS, including: direct brain parenchyma injections, systemic intravenous delivery using unique particles or conjugates that aid transport across the BBB, systemic intravascular injections with accompanied BBB disruption, and injections into the cerebrospinal fluid compartments (intra-CSF).

Of particular interest is the use of in vivo gene therapy for potentially providing a durable long-lasting treatment or cure for neurodegenerative diseases affecting the CNS. AAV vectors have emerged as the favored carrier for CNS in-vivo gene transfer because of their effectiveness in transducing CNS cells; their ability to produce persistent, long-term expression of the transgene in CNS cells (Hadaczek, Eberling et al. 2010); and their inherent safety. Wild-type AAV is not known to cause disease even though a number of AAV serotypes frequently infect humans. In addition, the transgene delivered with AAV vectors does not predominately integrate into the host genome (McCarty, Young et al. 2004, FDA 2006). This not only reduces the potential of carcinogenesis, but also reduces potential issues that may be caused by the mutation of a host gene. The AAV capsid is the smallest of the viral vectors being used in gene transfer today. This small capsid diameter, approximate 20 to 25 nm, may permit greater mobility through the narrow extracellular spaces of the brain, which have been measured to be 38 to 64 nm (Thorne and Nicholson 2006). The use of AAV vectors therefore provides a number of advantages for in vivo gene delivery to the CNS, and yet, AAV, like other biologic agents, have limited transport across the BBB and require alternative methods for entering the CNS and being broadly distributed within the CNS tissue.

CNS Intraparenchymal Delivery

The concept of using a hydraulic pressure higher than that of the tissue in order to cause flow of the fluid containing the desired agent is termed convection enhanced delivery (CED), which has been described in U.S. Pat. No. 5,720,720 by Laske et al., entitled "CONVECTION-ENHANCED DRUG DELIVERY," which issued on Feb. 24, 1998. This convection of biologic agents may result in a greater volume of distribution than that possible with diffusion alone, but the volume of distribution is still limited by the size of the particle, the affinity of the particles to cells within tissue, and the general reduction in the flow rate inversely proportional to the square of the distance from the injection site. Thus, the volume of cells sufficiently transduced by an injection of AAV vector is limited to a small volume surrounding the injection site.

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For example, without inducing damage to the tissue during the injection, the volume of cells sufficiently transduced surrounding each CED injection site resulting from CED injection of an AAV vector carrying genetic material has been shown to be less than one cm³ (Bobo, Laske et al. 1994, Burger, Nguyen et al. 2005) (Axonal retrograde transport has also been shown to increase the distribution of AAV depending on the site of injection.) AAV intraparenchymal injections have been able to achieve transduction in regions throughout the small brain volume of mice (0.7 cm³), but this method does not simply scale with brain size and results in the transduction of only a small percentage of the brain volume of larger animals and humans (approximately 1400 cm³ for humans). Linninger et al. (2008) and others have developed computer models intended to optimize CED distribution (Linninger, Somayaji et al. 2008, Linninger, Somayaji et al. 2008), but these attempts to significantly increase the transduced volume by modifying the CED injection parameters have not been successful in increasing the volume of distribution from a single injection site. AAV particle distribution with CED is limited by narrow and tortuous pathways within dense CNS tissue, by the size of the AAV particles, and most importantly, by the tissue binding characteristics of the AAV serotype (Chen, Hoffer et al. 2005).

The majority of previously conducted AAV gene transfer clinical trials for CNS diseases have used stereotactic positioned, brain parenchyma injections of the gene vector in order to bypass the BBB (Hocquemiller, Giersch et al. 2016). For example, the first two gene transfer clinical studies used brain intraparenchymal CED injections of AAV vectors for Canavan disease and Batten disease (Janson, McPhee et al. 2002, Crystal, Sondhi et al. 2004). While the biochemical effectiveness was demonstrated in preclinical studies on murine models of these diseases, neither of these studies showed significant clinical improvement of the patients. It is believed that a primary cause for these results was the inadequate distribution of the gene vectors to all of the affected CNS regions (Nagabhushan Kalburgi, Khan et al. 2013). In attempts by others to overcome this limitation, clinical studies have used up to 12 brain injection sites, but the total percentage of CNS tissue transduced is still estimated to be less than one percent of the total human brain volume. Adding a sufficient number of brain injection sites to cause global transduction of a human CNS is not an acceptable option because of the associated surgical risks of intraparenchymal injections.

To increase the volume of transduced CNS tissue, a number of groups have explored the use of a hyperosmotic fluid infusion to overcome the limited vector distribution with intraparenchymal injections (Burger, Nguyen et al. 2005, Carty, Lee et al. 2010). Burger et al. utilized an intravenous (IV) injection of mannitol in conjunction with brain intraparenchymal delivery of the viral vector (Burger, Nguyen et al. 2005). The results showed a statistical increase in CNS transduction. Even with this enhancement, the AAV dispersion from each injection site averaged only 4 mm³. Systemic Gene Delivery Targeting the CNS

Prior to reports in 2009 by Foust et al. and by Duque et al., systemic delivery of viral vectors was not considered a viable means of transferring genes to the CNS because of the limited transport of vectors across the BBB. These groups reported that intravenous (IV) delivery of self-complementary AAV serotype 9 (scAAV9) in mice and cats resulted in brain cell transduction including astrocytes, glia, and neurons proximal to brain vasculature (Duque, Joussem et al.

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2009, Foust, Nurre et al. 2009). Studies in mice conducted by Gray et al. (2009) have verified these results in mice (Gray, McCown et al. 2009).

Intravenous hyperosmotic solutions have also been used to increase the permeability of the BBB and aid the transfer of systemically delivered drugs to the CNS (Rapoport 2000). Although AAV serotype 2 does not normally pass through the BBB, Fu et al. (2003) reported the transduction of a small number of brain cells when an IV injection of self-complementary AAV serotype 2 (scAAV2) was preceded by an IV injection of mannitol. While this resulted in transduction of some cells within the brain, the level of transduction was significantly less than what could be obtained by direct injections into the CNS (Fu, DiRosario et al. 2010). More recently, Louboutin et al. reported that a significant increase in sv40-derived viral vectors (approximately 45 nm diameter) entered the CNS when administered systemically in mice 20 minutes after a large intraperitoneal injection of mannitol (3 ml of sterile 25% mannitol in 0.9% saline per 100 g body weight, e.g., ~7 g/kg mannitol).

Even though these IV methods of AAV delivery have demonstrated broad distribution within the CNS of mice and may scale to the human size anatomy, it has not yet been established whether the low level of cell transduction within the CNS will be adequate for treatment of a neurodegenerative disease in man. Another major consideration for IV delivery of AAV is that the high AAV vector dose required with IV delivery in humans is projected to be expensive and potentially toxic.

As an alternative to intravenous systemic delivery, Janson et al. (2014) has reported on the delivery of single-stranded AAVS vector directly to the carotid artery 60 seconds following a carotid artery injection of mannitol (~4 g/kg) (Janson, Romanova et al. 2014). Transgene expression occurred primarily on the ipsilateral side, and the procedure would need to be repeated on the contralateral side in order to achieve more global distribution. This BBB disruption method is similar to that first investigated by Stanley I. Rapoport (Rapoport 2000) and subsequently investigated for the delivery of gene vectors by others (Doran, Ren et al. 1995, Muldoon, Nilaver et al. 1995, Nilaver, Muldoon et al. 1995). While this localized delivery method has an advantage in both increasing the CNS uptake of the AAV vector and in reducing the required total dose for the AAV vector to sufficiently transduce cells within the CNS, it entails significantly more surgical risk than IV delivery of the hyperosmotic agent. Severe adverse events have been observed in clinical studies for the treatment of brain tumors using direct unilateral vertebral or carotid artery infusion with 25% mannitol at 5 to 12 mL/s for 30 seconds. These include non-reversible neurological damage (~1%) and seizures (~14%). One death was reported in a total of 630 procedures (Rapoport 2000).

Intra-CSF Gene Delivery

Prior studies using intraparenchymal CED have taken specific measures to avoid leakage of the therapeutic agents into the cerebrospinal fluid (CSF). It has been generally viewed that any therapeutic agent that leaks into the CSF will be "lost". On the other hand, while being less efficient, the delivery of AAV vectors into CSF using cerebroventricular, cisternal, or intrathecal spaces (intra-CSF) has been investigated in animal studies as a means of obtaining more global distribution. The results of these studies showed effective broad distribution in neonatal mice, while studies in older mice have resulted in low transduction efficiency generally limited to the ependymal tissue immediately adjacent to the CSF spaces (Davidson, Stein et al. 2000, Passini

and Wolfe 2001, Fu, Muenzer et al. 2003, Passini, Watson et al. 2003, Broekman, Comer et al. 2006, Watson, Bastacky et al. 2006). Similarly, studies conducted by Keimel et al. (reviewed in U.S. Pat. No. 8,419,710) showed that even a large protein, alpha-L-iduronidase (71 kDa), which is smaller than an AAV capsid, continuously infused or injected by bolus into the cisterna magna of dogs primarily distributed to the superficial cerebral cortex and the cerebellum (Keimel, Passage et al. 2006, Keimel and Kaemmerer 2013, Kakkis U.S. Pat. No. 7,442,372). It has been suggested that the scattered and inconsistent transduction patterns using intra-CSF delivery are explained by the directional flow of brain interstitial fluid outward from the parenchyma and the limited diffusion of large particles to overcome this flow (Rosenberg, Kyner et al. 1980, Chen, Hoffer et al. 2005).

In 1999, Ghodsi et al., reported that transient systemic hyperosmolarity at the time of an intracerebroventricular (ICV) injection of an adenoviral vector would somewhat enhance the penetration of the vector across the ependymal cell layer in mice (Ghodsi, Stein et al. 1999). Similarly, in 2000, Leone et al. reported the experiences in rats and two patients of ICV injections of a non-viral lipid-entrapped, polycation-condensed delivery system (LPD), which were preceded by systemic mannitol (1 g/kg) intended to increase interstitial permeability (Leone, Janson et al. 2000). The authors qualitatively reported that the most intense transduction in the vicinity of the ependymal and subependymal cells in the ventricular spaces. Haiyan Fu et al., at the University of North Carolina, subsequently conducted a similar study that used AAV vectors delivered to the cisterna magna of mice. This study showed enhanced distribution of transduced cells when the AAV vectors were injected 20 minutes after an IV pre-treatment of 100 μ L of 25% mannitol (approximately 1 g/kg body weight). This study illustrated the comparison of GFP expression with and without the pre-treatment of IV mannitol (Fu, Muenzer et al. 2003). More recent studies by this same group demonstrated that a single intracisternal injection of AAV vector with a pretreatment of IV mannitol had a significant neurological benefit in adult mucopolysaccharidosis IIIB mice (Fu, DiRosario et al. 2010). In gene transfer research using a single-stranded AAV vector injected into the cerebral ventricles of homozygous mucopolysaccharidosis type-1 mice, Janson et al. compared the transduction efficacy of the vector with systemic or ICV administration of mannitol. Both the systemic and the ICV co-administration of the mannitol with the ICV AAV injections were superior to the ICV AAV injections without co-injection of mannitol, which resulted mainly in expression within the choroid plexus and along the needle tract.

Methods have not previously been identified for the delivery and broad distribution of large particle biologic agents throughout the brain and spinal cord tissue of large animals and humans. Convective transport characteristics and the BBB permeability are major considerations in the development of these methods for large animals and humans. A simple, safe, and effective means of achieving broad distribution of biologic agents is needed to enable biologic agents to be effective in treating diffuse CNS diseases.

Brain Vasculature and the Blood Brain Barrier

The influence of systemic hyperosmotic agents on enhancing gene delivery requires an understanding of the anatomical aspects of the CNS vasculature and the role of the semipermeable membrane between the blood and the parenchyma interstitial fluid (ISF). The cranium blood macro- and micro-vessels together occupy a significant (25

to 30%) of the total brain volume with a surface area of approximately 12 square meters for humans (Zhang, Inman et al. 1990). With every brain cell located within 20 μ m of a capillary, delivery across the walls of these vessels is a logical means of globally transferring a drug agent throughout the CNS. But as described above, the blood vessels within the brain are composed of tight-junctioned endothelial cells and are further surrounded by a thin basal lamina that combine to form the blood-brain barrier (BBB). The vessel walls also contain contractile pericyte cells that serve to control blood flow through the vessels. Closely spaced astrocyte end feet further surround the intracerebral blood vessels. The endothelial cell tight junctions have been shown to contain a number of proteins, including membrane-spanning glycoproteins called cadherins, which limit paracellular transport (Rapoport 2000). Under normal conditions, the passage of drugs through the BBB has been shown to be directly related to lipid solubility (octanol-water partition coefficient, Log $P_{octanol}$) (Habgood and Ek 2010).

Interstitial Fluid

The brain is a dense tissue and this further limits the distribution of large particles within the parenchyma. The brain parenchyma extracellular space has been estimated to have a normal width of 38 to 64 nm (Thorne and Nicholson 2006). The size of this extracellular space and the tortuosity of the grey matter cell structure restrict diffusion and can also restrict the convective movement of particles as the size of the particles approach the size of the extracellular space. The particle outer dimensions are therefore a factor for both the diffusion and the convection within the brain.

The surface area of cerebral capillary endothelium is approximately 100 cm^2 per gram of brain tissue (Zhang, Inman et al. 1990), and this large surface area, even with its tight junctions, accounts for substantial fluid seepage into the brain. This flow across the BBB, plus the water created by the glycolysis of glucose within brain cells, is the source of interstitial fluid (ISF). A portion of this ISF drains into the CSF compartments.

Perivascular spaces, as illustrated in FIG. 3, surround both veins and arteries from the subarachnoid spaces down to the level of arterioles and venules, but not down to the capillaries (Pullen, DePasquale et al. 1987). The ISF normally drains from the brain to the CSF through a network of fluid channels, which include these perivascular spaces. These brain extracellular spaces are in fluid contact with the CSF through porous openings in the pia layer. Large protein molecules readily cross the pia. In general, the flow of a fluid through the porous brain parenchyma can be modeled by Darcy's law: $v=K\nabla p$, where v is the fluid velocity vector, K is the hydrostatic conductivity tensor, and ∇p is the hydrostatic pressure gradient; but, a more detailed analysis may be required to account for the perivascular fluid channels.

Cerebral Spinal Fluid

CSF is a product of both the secretion of the ventricular choroid plexus and the ISF drainage from the parenchyma tissue, as noted above (Weed 1914, Pullen, DePasquale et al. 1987). It has been estimated that two thirds of the total CSF is secreted by the choroid plexuses (Johanson, Duncan et al. 2008). The ISF secretion rate at the BBB is substantially slower (1/100 when normalized for surface area) than the CSF secretion from the choroid plexus, but because of the large BBB surface area, a significant percentage of CSF originates from the ISF. The CSF drains out of the CNS into both the blood through the arachnoid villa and into the lymph along the cranial nerves and the spinal nerve root ganglia. A large percentage of protein injected into CSF has been shown to pass into the lymph (Cserr and Knopf 1992).

CSF Flow in Response to Hydrostatic Pressure

An oscillatory movement of CSF occurs in response to pulsatile cardiac pressure (Greitz 1993). With cardiac systole, intracranial blood vessels expand, and CSF is forced out of the ventricles and cranial subarachnoid spaces and moves into a compliant portion of the lower spinal intrathecal space. This CSF flow is then reversed during diastole. By itself, this oscillatory movement does not result in net flow of CSF, but does provide limited CSF mixing. With this, the fourth ventricle and the cisterna magna, in particular, serve as CSF mixing chambers (Enzmann and Pelc 1991).

Normally, the average CSF hydrostatic pressure is equal to the cerebral venous pressure minus the elastic forces of the venous walls. The response to mechanically induced, incremental changes in the CSF hydrostatic pressure was investigated by Noell and Schneider (Davson and Segal 1996). They found that incrementally raising the cisternal hydrostatic pressure resulted in a corresponding increase in intracranial venous pressure. This is as one would expect. Gradually raising the intracranial pressure (ICP) above that of the blood vessels will cause a collapsing force on the vessels, but the vis a tergo of the arterial blood will in-turn cause the capillary pressure to rise thereby preventing vessel collapse and maintaining blood flow. It has also been shown by Harvey Cushing in 1902 that as the CSF hydrostatic pressure is raised above the arterial systolic blood pressure, an autoregulatory response occurs, now known as the Cushing Reflex, that elevates the blood pressure and maintains blood flow to the brain (Cushing 1902). Therefore, not even large induced increases in the ICP will result in a steady state pressure gradient across the BBB.

The drainage (absorption) of CSF into both the arachnoid villa and lymphatic pathways has been shown to be linearly related to ICP (Cutler, Page et al. 1968, Boulton, Armstrong et al. 1998). This relationship is termed the resistance to absorption. Increasing ICP will cause a corresponding increase in bulk CSF flow towards the arachnoid villa and areas of lymphatic drainage.

Osmotic Flow Across the Blood-Brain Barrier

As noted above, a systemic infusion of a hyperosmotic solution has been shown to increase the CNS distribution of intra-CSF and IV delivered viral vector particles. The intra-CSF delivery methods may benefit from brain ISF flow arising from osmotic 'water' flow across the BBB. On the other hand, a systemically delivered vector may also require a sufficient disruption in the BBB to enhance passage of viral capsids into the brain.

Systemic delivery of a hyperosmotic solution is known to have an effect on the bulk flow of ISF. Rosenberg et al. studied the normal flow rate of ISF and the flow after systemic infusion of mannitol in both gray and white matter of cats. Under normal conditions, ISF flow was negligible in gray matter, but the ISF flowed toward the ventricles at a rate of 10.5 $\mu\text{m}/\text{min}$ in white matter. Four hours following the start of a 30 minute IV infusion of 20% mannitol (1.5 to 3 g/kg), the bulk flow of ISF in gray matter changed direction away from the ventricles (Rosenberg, Kyner et al. 1980).

The brain vasculature can be considered a semipermeable membrane due to the restrictions imposed by its tight-junctioned endothelial cells. The Starling equation relates the flow across a semipermeable membrane to the hydrostatic pressure and osmotic pressure differences across the membrane:

$$f = ALp(\Delta P - \sigma \Delta \Pi)$$

where f is the flow across the membrane, A is the membrane area, L_p is the hydrostatic or filtration coefficient, ΔP is the hydrostatic pressure across the membrane, σ is the reflection coefficient, and $\Delta \Pi$ is the osmotic pressure. The osmotic pressure can be further modeled using van't Hoff's law:

$$\Delta \Pi = RT \Delta C$$

where R is the gas constant, T is the absolute temperature, and ΔC is the combined osmolarity difference of solutes across the membrane (Osm/L). Under normal conditions, the osmolality of the human cerebrospinal fluid is between 280 and 300 mOsm/kg of H_2O . Osmolarity is the amount of the total osmoles of all solute per liter of solution, whereas osmolality (with an "l") is the measure of the total osmoles of all solutes per kilogram of solvent. Blood typically has an osmolality between 275 and 295 mOsm/kg. The normal intracranial pressure (ICP) is 5 to 15 mmHg (or 7 to 20 cmH_2O). An equivalent intracerebral venous pressure must counter this ICP in order to maintain patency of the vessels. The cranium and spinal column space can be simplistically modeled, as shown in FIG. 1.

When the osmolarity of the intracranial blood is increased, an osmotic pressure develops across the BBB. As reflected in Starling's equation, this results in a net flow, primarily water, through the BBB into the blood. If this flow is greater than the CSF synthesis rate, the total volume of ISF and CSF will decrease. This, in turn, will increase the solute concentration of the ISF and CSF and also reduce the intracranial pressure. Both of these factors will offset the initial osmotic force for flow across the BBB. Also to be considered is the Monro-Kellie hypothesis that states that the cranium has a fixed volume and that the total volume of brain parenchyma, the CSF, and the cerebral blood must remain nearly constant. Therefore, a reduction in the volume of ISF and CSF must be, at least transiently, offset by an increase in the cranial blood volume. Volume homeostasis will eventually return by either BBB backflow from the cerebral capillaries or by CSF synthesis.

Methods and Systems

In consideration of the preceding points, embodiments herein can include a method of administering a therapeutic agent to the central nervous system (CNS) including steps of injecting a therapeutic agent into a first cerebrospinal fluid (CSF) region of the subject, establishing fluid communication between a fluid reservoir and a second cerebrospinal fluid (CSF) region of a subject and infusing a hyperosmotic fluid systemically.

The hyperosmotic fluid causes an osmotic pressure across the BBB, resulting in a net flow of fluid outward across the BBB. This fluid flow can, in turn, cause the therapeutic agent to be transported from the injection site in a CSF region into the parenchyma and ISF thereof through convection. The fluid reservoir, in fluid communication with a CSF region, can serve as a source of fluid and be drawn into the CSF region in order to replace the volume of fluid carrying the therapeutic agent and moving from the CSF region and into the parenchyma and ISF thereof.

As such, the fluid coming from the fluid reservoir prevents the pressure within the CSF region from dropping to a level that would inhibit further movement of fluid from the CSF region and into the parenchyma and ISF thereof. This is because in the absence of fluid being drawn in from the fluid reservoir, osmotic induced flow across the BBB reduces ISF volume, but with a low CSF synthesis rate and keeping with the Monro-Kellie Hypothesis, the volume of cerebral blood would have to increase so that the total CNS volume remains constant. This expansion of the volume of cerebral blood

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would happen at least partially in lieu of further fluid movement across the BBB and thus would inhibit further convection of the therapeutic agent.

The method can specifically include injecting a therapeutic agent into a first cerebrospinal fluid (CSF) region of the subject. It will be appreciated that the injection can be accomplished in various ways. In some embodiments a cannula or needle can be used to inject the therapeutic agent.

In some embodiments, the method can include establishing fluid communication between a fluid reservoir and a second cerebrospinal fluid (CSF) region of a subject. It will be appreciated that fluid communication can be established in various ways and using various pieces of equipment. In various embodiments, the fluid having a hydraulic pressure at or above an intracranial pressure. In some embodiments, the method can further include inserting a conduit to provide fluid communication between the reservoir and the second CSF region of the subject. In some embodiments, the method can further include infusing a hyperosmotic fluid systemically.

The various steps of methods herein can be performed in various specific orders. In some embodiments, the step of injecting the therapeutic agent into the first cerebrospinal fluid (CSF) region of the subject is performed before, during or after the step of infusing the hyperosmotic fluid systemically. In some embodiments, the step of injecting the therapeutic agent into the first cerebrospinal fluid (CSF) region of the subject is performed before the step of infusing the hyperosmotic fluid systemically. In some embodiments, the gap in time between injecting the therapeutic agent and beginning infusion of the hyperosmotic fluid systemically (regardless of which comes first) can be approximately 0 seconds, 0 to 30 seconds, 30 to 60 seconds, 1 minute to 2 minutes, 2 minutes to 3 minutes, 3 minutes to 4 minutes, 4 minutes to 6 minutes, 6 minutes to 10 minutes, 10 minutes to 15 minutes, or 15 minutes to 20 minutes or more.

Referring now to FIG. 4, a schematic diagram of a system 400 in accordance with various embodiments herein. The system 400 can include components for the execution of various steps in accordance with methods herein. The system 400 can be effective to administer a therapeutic agent to the central nervous system (CNS) of a subject 402. While the subject 402 shown in FIG. 4 is non-human, it will be appreciated that in various embodiments the subject can be a human. The subject 402 can include a CNS 404. The subject 402 can include a first CSF space 406 and a second CSF space 408.

The system 400 can further include an instrument 412 to deliver or inject an active agent, such as a syringe or similar instrument, to a first CSF space 406.

The system 400 can further include a reservoir 414 including an isotonic or hypotonic liquid, including but not limited to, a synthetic or artificial cerebrospinal fluid. The reservoir 414 can be in fluid communication with a second CSF space 408 via a conduit 416. The conduit 416 can provide a sterile means of transporting the fluid from the reservoir 414 to the second CSF space 408.

In some embodiments, a measurement device 426 for measuring pressure can be included. For example, the measurement device 426 can be a liquid column manometer. However, other devices for measuring pressure are contemplated herein. With use of a liquid column manometer, the height of the fluid in the CSF reservoir 414 can be adjusted to be at or above the height of the fluid in the manometer. It will be appreciated that the measurement device 426 could also take alternative forms, such as a pressure gauge.

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A stopcock 428 (such as a three-way stopcock) can be included to selectively block or provide fluid communication with any of the inputs thereto (e.g., the device 426 for measuring pressure and the reservoir 414) and the output therefrom (e.g., conduit 416). For example, the stopcock can be actuated to selectively provide fluid communication between the device 426 for measuring pressure and the conduit 416 and second CSF space 408, while temporarily blocking fluid communication with the reservoir 414. This can allow for the specific measurement of pressure in the area of the second CSF space 408.

In some embodiments, a load cell 430 (or other type of device capable of measuring or being responsive to changes in weight) can be used to monitor the amount of fluid and/or the change in the amount of fluid in the reservoir 414. In some embodiments the load cell 430 can provide a read-out to recording equipment so as to document the rate and total fluid amount entering the CSF. In some embodiments, data from the load cell 430 can also be used to provide an indication as to when the procedure is complete. As merely one illustrative example, one could decide that sufficient convection of the therapeutic agent has occurred when 50 cc of CSF fluid from the reservoir has entered the CNS (wherein a one gram change in the CSF fluid weight is approximately equal to one cc of fluid entering the CNS.)

In some embodiments, an alternative access port 438 can be included. The alternative access port 438 can be used for injections and, in some cases, can be used for the injection of a therapeutic agent, such as those described herein.

The reservoir 414 can be suspended from (or otherwise attached to) an adjustable shepherd hook stand 422. The height of the adjustable shepherd hook stand 422 can be adjusted as shown by arrow 424. Adjusting the height of the adjustable shepherd hook stand 422 can allow for adjustment of the pressure of the fluid in the reservoir 414.

In various embodiments, the conduit 416 can be an intrathecal catheter or can at least include components of the same. In various embodiments, the conduit 416 can include tubing material such as polyvinylchloride (PVC), polyethylene, polyurethane, polyamide, silicone, synthetic rubber, and the like. An exemplary intrathecal catheter is described in US Publ. Appl. No. 2008/0140008, the content of which is herein incorporated by reference. In various embodiments, the conduit can include a cannula. The interior diameter of the conduit can be sufficiently large so as to avoid creating a relatively large pressure drop between the reservoir and the end of the conduit 416 where it provides fluid communication with the second CSF space 408.

The system 400 can include a reservoir 410 including a hyperosmotic liquid to be infused systemically to the subject 402. Details of exemplary hyperosmotic liquids are described in greater detail below. The reservoir 410 for the hyperosmotic liquid can be associated with an infusion pump 434 and an infusion pump stand 432. The hyperosmotic liquid can be delivered to the subject 402 from the infusion pump 434 systemically through an infusion line 436 or conduit. However, other means of providing for infusion of the hyperosmotic fluid are also contemplated herein. Therapeutic Agents

Various therapeutic agents can be administered in accordance with embodiments herein. In some embodiments, the therapeutic agent can be small molecule therapeutic agent. In other embodiments, the therapeutic agent can be a non-small molecule therapeutic agent, such as biologics. Therapeutic agents can include, but are not limited to, gene therapy agents, proteins (including, but not limited to, natural proteins, recombinant therapeutic proteins, antibodies,

and the like), sugars, nucleic acids (including, but not limited to, natural nucleic acids, recombinant nucleic acids, vectors, and the like) and combinations of the same. Vectors can include, but are not limited to, plasmids, viral vectors, cosmids, and artificial chromosomes.

In some embodiments, the therapeutic agent can include a polynucleotide. In some embodiments, the therapeutic agent can include a recombinant polynucleotide. In some embodiments, the therapeutic agent can include a vector comprising a recombinant polynucleotide, including but not limited to vectors described above.

In some embodiments, the therapeutic agent can include a viral vector comprising a recombinant polynucleotide, including but not limited to vectors described above. Viral vectors can include, but are not limited to, recombinant retroviruses, recombinant lentiviruses, recombinant adenoviruses, and recombinant adeno-associated viruses. In some embodiments the therapeutic agent can specifically include an adeno-associated virus (AAV) vector.

While not intending to be bound by theory, it is believed that AAV vectors can be beneficial because AAV is highly efficient at transducing CNS cells; AAV vectors have demonstrated long-term (>8 years) expression in the CNS; AAV vectors have a small viral capsids with a diameter of 20 to 25 nanometers allowing better passage within the brain extracellular space. In addition, wild-type AAV is not known to cause disease and the transgene delivered from an AAV vector generally does not integrate into the host genome, which reduces concern of carcinogenesis.

In some embodiments, the therapeutic agent can include at least one selected from the group of proteins (including recombinant proteins and antibodies), anti-sense RNA, siRNA, and RNAi.

The specific dosages of the therapeutic agents can vary based on the nature of the condition to be treated and the activity of the therapeutic agent itself. In various embodiments, a therapeutically effective amount of the therapeutic agent is administered.

The therapeutic agent can be formulated with a carrier in order to provide sufficient volume for effective delivery. It will be appreciated that many different carriers can be used. In various embodiments, the carrier is an isotonic liquid, such as an isotonic aqueous liquid. The carrier can include various salts, sugars, sugar alcohols, and other compounds including, but not limited to, buffers. In some embodiments, the active agent carrier fluid can include the same components as described elsewhere herein regarding artificial or synthetic CSF fluid. The total volume of the therapeutic agent and the carrier liquid can be sufficient to allow for ease of injection at the desired site.

CSF Spaces

As described above, in various embodiments a therapeutic agent is injected or otherwise administered to a first CSF region or space. In addition, fluid communication is established between a second CSF region or space and a fluid reservoir. Cerebrospinal fluid (CSF) is a clear, colorless body fluid found in the brain and spine. The CSF occupies the subarachnoid space (between the arachnoid mater and the pia mater) and the ventricular system (a set of four interconnected cavities or ventricles in the brain). It constitutes the content of the ventricles, cisterns and sulci of the brain, as well as the central canal of the spinal cord. As used herein the term "CSF region" or "CSF space" shall refer to the region of a subject's anatomy that, under normal circumstances, is filled with cerebrospinal fluid.

It will be appreciated that the first CSF region (the region where the therapeutic agent is injected or otherwise admin-

istered) and the second CSF region (the region that is in fluid communication with the fluid reservoir) can be different physical locations. However, in some embodiments, the first CSF region and the second CSF region can be the same physical location. For example, in some embodiments, the area where the therapeutic agent is injected or administered can be the same general area that where fluid communication is established with the fluid reservoir and in other embodiments those two areas can be different.

In some embodiments, the first and second CSF regions can be selected from the group consisting of the cerebroventricular, cisternal, or intrathecal spaces (including, but not limited to the lumbar intrathecal space).

In some embodiments, the area where the therapeutic agent is injected or otherwise administered (first CSF region), is selected from the group consisting of the cerebroventricular and cisternal spaces. In some embodiments, the therapeutic agent can be injected simultaneously or sequentially in multiple different sites.

In some embodiments, the area where fluid communication is established with the fluid reservoir (second CSF region) is the intrathecal space (including, but not limited to the cisternal and/or lumbar intrathecal space). In some embodiments, fluid communication between the CSF region(s) and the fluid reservoir can be at multiple different sites.

Fluid Reservoir and Fluids

In some embodiments, the fluid reservoir includes a fluid that can be drawn from the reservoir and into the second CSF region. The fluid can include various biocompatible fluids. The fluid can include various dissolved solutes therein in various concentrations. In some embodiments, the fluid in the fluid reservoir can be isotonic or hypotonic. While not intending to be bound by theory, in view of a desired to create a current across the blood brain barrier, it is believed that the use of isotonic or hypotonic fluids in the fluid reservoir can be more effective than hypertonic fluids.

In some embodiments, the fluid reservoir can include a fluid having an osmolality of less than or equal to about 300, 295, 290, 285, 280, 275, 270, 265, 260, 255, 250, 245, 240, 235, 230, 225, 220, 210, 200, or 190 mOsm/kg H₂O. In some embodiments, the fluid can have an osmolality in a range wherein any of the foregoing values can serve as the upper or lower bound of the range, provided that the upper bound is greater than the lower bound. In a particular embodiment, the fluid reservoir can include a fluid having an osmolality of less than or equal to about 285 mOsm/kg H₂O.

In some embodiments, the fluid reservoir can include an aqueous saline solution as the fluid. In some embodiments, the aqueous saline solution can include from about 0.6% (by weight) to about 1.2% (by weight) saline. In some embodiments, the fluid can be about 0.9% saline. In some embodiments, the fluid can be a lactated Ringer's solution. In some embodiments an artificial or synthetic cerebrospinal fluid. Many different specific formulations for artificial or synthetic cerebrospinal fluids are contemplated. In one example, 119 mM NaCl, 26.2 mM NaHCO₃, 2.5 mM KCl, 1 mM NaH₂PO₄, 1.3 mM MgCl₂, 10 mM glucose are mixed (in those proportions, but with the total amounts dictated based on the desired final value for mOsm/kg H₂O). This mixture can then be sparged with a gas mixture of 5% CO₂/95% O₂ for 10-15 min, then 2.5 mM CaCl₂ can be added (again, as proportioned based on the desired final value for mOsm/kg H₂O). Synthetic or artificial cerebrospinal fluid are also available commercially, such as from Tocris Bioscience, Bristol U.K (Cat. No. 3525).

In some embodiments, the fluid reservoir can initially contain an amount of fluid sufficient to accommodate an expected amount of fluid to be drawn into the second CSF region, allowing for some reasonable safety factor. In some embodiments, the fluid reservoir contains an amount of fluid equivalent to at least about 10, 15, 20, 25, 30, 35, 40, or 45% or more of the subject's total cerebrospinal fluid. In some embodiments, the fluid reservoir contains an amount of fluid equivalent to at least about 25% of the subject's total cerebrospinal fluid. The following table (Table 1) shows approximate cerebrospinal fluid volumes for a variety of species of possible subjects.

TABLE 1

Common Name	Body Weight (kg)	CSF Volume (ml)	CSF Synthesis (ml/h)	Brain (g)	Scale-up from Mouse
Mouse	0.025	0.035	0.018	.7	1
Rat	0.3	0.275	0.18	2	3
Cat (domestic)	4	5	1.2	30	50
Dog (beagle)	20	50	3	70	100
Sheep	40	35 to 50	4 to 11	140	200
Human (newborn)	4	50	—	350-400	500
Human (adult)	70	150	20-30	1300-1400	2000

In some embodiments, the fluid reservoir can contain at least about 10, 20, 30, 40, 50, 60, 70, 80, 90, 100, 110, 120, 130, 140, 150, 160, 170, 180, 190, 200, 210, 220 ml or more of fluid.

In some embodiments, the fluid in the fluid reservoir can be maintained so as to have a hydraulic pressure at or above the baseline intracranial pressure. In particular, the fluid in the fluid reservoir can be maintained such that at the point wherein the fluid is drawn into the second CSF region, the hydraulic pressure is maintained at or above a baseline intracranial pressure.

In some embodiments, the fluid in the fluid reservoir can be maintained so as to have a hydraulic pressure at or above a central venous pressure. In particular, the fluid in the fluid reservoir can be maintained such that at the point wherein the fluid is drawn into the second CSF region, the hydraulic pressure is maintained at or above a central venous pressure.

In some embodiments, the fluid can be maintained so as to have a hydraulic pressure from about 5 cm to about 20 cm H₂O or from about 10 cm to about 15 cm H₂O above central venous pressure, and at or above the baseline intracranial pressure.

While not intending to be bound by theory, it is believed that it can be detrimental if the fluid is maintained at a hydraulic pressure that is too high above intracranial pressure. In specific, higher pressures can lead to accelerating losses of CSF fluid from drainage via the arachnoid villa.

It will be appreciated that the hydraulic pressure of the fluid within the fluid reservoir can be maintained and/or elevated in various ways. By way of example, in some embodiments, the reservoir is physically elevated to increase the hydraulic pressure of the exogenous cerebrospinal fluid. In some embodiments, a pump can be included. The pump can be in fluid communication with the reservoir and the pump can serve to increase the hydraulic pressure of the fluid within the reservoir.

Hyperosmotic Fluids

A hyperosmotic fluid can be infused systemically. In some embodiments, the hyperosmotic fluid can have an osmolality of greater than about 400, 500, 600, 700, 800, 900, 1000, 1100, 1200 or 1300 mOsm/kg H₂O. In some embodiments, the hyperosmotic fluid can have an osmolality in a range wherein any of the foregoing amounts can serve as the upper or lower bound of the range. In some particular embodiments, the hyperosmotic fluid can have an osmolality of greater than about 1000 mOsm/kg H₂O.

The hyperosmotic fluid can include various solutes. In some embodiments, the hyperosmotic fluid can include a sugar alcohol as a solute. In some embodiments, the hyperosmotic fluid can include at least one of mannitol and arabinose in an aqueous solution. In some embodiments, the hyperosmotic fluid can include 10, 15, 20, or 25 wt. % or more mannitol.

The amount (dose) of the hyperosmotic fluid infused can vary. For example, in the context of mannitol, a dose can be infused of at least about 0.5, 1.0, 1.5, 2.0, 2.5, 3.0, 3.5, 4.0, 4.5, 5.0, 5.5, or 6.0 g mannitol per kg of body weight. In some embodiments, a dose of mannitol is infused in the range of about 0.5 g mannitol per kg of body weight and 4 g mannitol per kg of body weight.

The dose of hyperosmotic fluid can be infused over various time frames. In some embodiments, the dose can be infused over a period of 5, 10, 15, 20, 25, 30, 35, 40, 45, 50, 60, 70, 80, or 90 minutes. In some embodiments, a dose of mannitol is infused over a time period of 10 to 30 minutes.

The specific site for infusion of the hyperosmotic fluid can vary. In some embodiments, the hyperosmotic fluid is infused into the carotid artery. In some embodiments, the hyperosmotic fluid is infused intravenously. Other sites for infusion are also contemplated herein.

Kits

In various embodiments, a kit is included herein. The kit can include any of the components described above. The kit can include some or all of the components for executing a method described herein. In some embodiments, the kit can include a first reservoir, a first fluid configured to be disposed within the first reservoir. The first fluid can be such as those described above. In some embodiments, the first fluid can be isotonic or hypotonic. The kit can further include an instrument for injecting a therapeutic agent into a first CSF space. Examples of suitable instruments are described above. The kit can further include a conduit for providing fluid communication between the first reservoir and a second CSF space. In some embodiments, the conduit can be an intrathecal catheter. The kit can further include a second reservoir and a second fluid configured to be disposed within the second reservoir. The second fluid can be as those described above. The second fluid can be hyperosmotic.

In various embodiments, a system is included herein. The system can include any of the components described above. The system can include some or all of the components for executing a method described herein. For example, in an embodiment, a system is included having a first reservoir and a first fluid disposed within the first reservoir, wherein the first fluid is isotonic or hypotonic. The system can further include a conduit for providing fluid communication between the first reservoir and a second CSF space. The system can further include a second reservoir and a second fluid disposed within the second reservoir, wherein the second fluid is hyperosmotic.

It should be noted that, as used in this specification and the appended claims, the singular forms "a," "an," and "the" include plural referents unless the content clearly dictates

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otherwise. Thus, for example, reference to a composition containing “a compound” includes a mixture of two or more compounds. It should also be noted that the term “or” is generally employed in its sense including “and/or” unless the content clearly dictates otherwise.

It should also be noted that, as used in this specification and the appended claims, the phrase “configured” describes a system, apparatus, or other structure that is constructed or configured to perform a particular task or adopt a particular configuration to. The phrase “configured” can be used interchangeably with other similar phrases such as arranged and configured, constructed and arranged, constructed, manufactured and arranged, and the like.

All publications and patent applications in this specification are indicative of the level of ordinary skill in the art to which this invention pertains. All publications and patent applications are herein incorporated by reference to the same extent as if each individual publication or patent application was specifically and individually indicated by reference.

Aspects have been described with reference to various specific and preferred embodiments and techniques. However, it should be understood that many variations and modifications may be made while remaining within the spirit and scope herein.

The invention claimed is:

1. A method of administering a therapeutic agent to a central nervous system (CNS) of a subject comprising:

injecting a therapeutic agent into a first cerebrospinal fluid (CSF) region of the subject;

the therapeutic agent comprising a biologic agent;

establishing fluid communication between a fluid reservoir and a second cerebrospinal fluid (CSF) region of the subject, a fluid within the fluid reservoir having a hydraulic pressure maintained at a baseline intracranial pressure; and

infusing a hyperosmotic fluid systemically.

2. The method of claim 1, the first and second CSF regions selected from the group consisting of the cerebroventricular, cisternal, or intrathecal spaces.

3. The method of claim 1, wherein the first CSF region selected from the group consisting of the cerebroventricular and cisternal spaces.

4. The method of claim 1, wherein the second CSF region comprises an intrathecal space.

5. The method of claim 1, the fluid reservoir comprising a fluid that is isotonic or hypotonic.

6. The method of claim 1, the fluid reservoir comprising a fluid selected from the group consisting of 0.9% saline, lactated Ringer's solution, and a synthetic cerebrospinal fluid.

7. The method of claim 1, further comprising maintaining the fluid in the fluid reservoir to have a hydraulic pressure

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from about 5 cm to about 20 cm H₂O above central venous pressure, and at the baseline intracranial pressure.

8. The method of claim 1, wherein fluid is drawn across the blood brain barrier and out of the brain by osmotic pressure.

9. The method of claim 1, the hyperosmotic fluid having an osmolality of greater than about 1000 mOsm/kg H₂O.

10. The method of claim 1, the therapeutic agent comprising a polynucleotide.

11. The method of claim 1, the therapeutic agent comprising a vector comprising a recombinant polynucleotide.

12. The method of claim 1, the therapeutic agent comprising an adeno-associated virus (AAV) vector.

13. The method of claim 1, the therapeutic agent comprising at least one selected from the group consisting of antibodies, proteins, anti-sense nucleic acids and RNAi.

14. The method of claim 1, the therapeutic agent comprising a non-small molecule agent.

15. The method of claim 1, further comprising a pump in fluid communication with the fluid reservoir, wherein the pump increases the hydraulic pressure of the fluid within the fluid reservoir.

16. The method of claim 1, wherein the fluid reservoir is physically elevated to increase the hydraulic pressure of the fluid within the fluid reservoir.

17. The method of claim 1, further comprising inserting a conduit to provide fluid communication between the fluid reservoir and the second CSF region of the subject.

18. The method of claim 17, the conduit comprising an intrathecal catheter.

19. The method of claim 1, wherein the step of injecting the therapeutic agent into the first cerebrospinal fluid (CSF) region of the subject is performed before or during the step of infusing the hyperosmotic fluid systemically.

20. A method of administering a therapeutic agent to a central nervous system (CNS) of a subject comprising:

injecting a therapeutic agent into a first cerebrospinal fluid (CSF) region of the subject, the therapeutic agent comprising a polynucleotide;

inducing convective flow to transport the therapeutic agent directly from the first CSF region into the parenchyma by:

establishing fluid communication between a fluid reservoir and a second cerebrospinal fluid (CSF) region of the subject, a fluid within the fluid reservoir having a hydraulic pressure maintained at a baseline intracranial pressure; and

infusing a hyperosmotic fluid systemically.

21. The method of claim 20, wherein the first CSF region and the second CSF region are different.

22. The method of claim 20, wherein the first CSF region and the second CSF region are the same.

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